



Plasma Nanotechnologies for Cardiovascular Implants



Artificial blood vessel

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Classical technologies for materials processing run close to thermal equilibrium



Rather high temperature is required for chemical reactions



Materials can be damaged before achiving certain effects







Q: Is it possible to avoid high temperature?

Heating of materials by gas depends on the gas temperature

Chemical reactivity of oxygen depends on the concentration of molecules in excited states

$$\frac{N_a}{N} = e^{-\frac{W(kT)}{kT}}$$







Nature does not allow high density of excited states at low gas temperature

Avoid the basic law of thermodynamics!









Q: How do we avoid thermodynamics?

A: Do not create highly excited states by heating of gas.

Use free electrons instead

Free electrons are capable to excite molecules without heating them!







Electrons cannot heat gas (transfer kinetic energy to a molecule) due to the small mass

Elastic collision





 $W_k = \frac{1}{2} M v^2 \rightarrow$ Kinetic energy of heavy molecule is negligible

ELECTRONS EXCITE MOLECULES EASILY BUT NOT HEAT THEM





Q: How do we create gas with substantial amount of free electrons?

A: In an electrical discharge













Applications

Activation of polymers for better adhesion (painting, printing)





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Discharge cleaning

Sterilization





Plasma 486

Synthesis of nanoparticles











Cardiovascular diseases represent the major cause of death in wealthy countries



Only in USA, the costs annual exceed 500 billion \$



Learn and Live "



stress

improper diet





Curing of cardiovascular diseases is by surgery



Vascular grafts

Graft is pushed out of the catheter

stents





A common post-surgery complication is thrombosis

Coagulation cascade



Fibrinogen to fibrin fibres



fibrin fibres form a network capturing erythrocytes



http://www.ldeo.columbia.edu/micro/im ages.section/pages/bloodclot.html





Fibrin fibres accommodate quickly upon incubation of an artificial blood vessel with blood





Vascular grafts are made from knitted polymers, often PET





Coagulation cascade is stimulated by platelet activation





Platelets' shape change upon activation





Activation of blood platelets on polymer surface is due to insufficient biocompatibility

Possible solutions:

Coat with heparin

Gaseous plasma treatment

Make the contact area minimal by nano-structuring





Platelets spread on <u>smooth</u> surface of polymer

Minimize the contact area!

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PET substrate





platelet PET substrate

Contact area is minimized by making substrate rough on sub-micron scale

PET polymer for vascular grafts is semi-cristalline



amorphous

crystallites



SELECTIVELY ETCH THE AMORPHOUS PHASE AND YOU WILL MAKE MATERIAL ROUGH ON SUB-MICRON SCALE











Reactive oxygen species cause low-temperature "burning" of polymer

> Etching rate depends on crystallinity (nm/s)





SEM image -

optimal

roughness

Non – equilibrium oxygen plasma is an excellent medium for selective etching of carbon-containing materials

AFM image of plasma treated originally smooth semicristalline PET foil





Surface morphology changes upon plasma treatment







Plasma radicals readily interact chemically with the surface of organic materials



O – atoms are incorporated into the surface layer of polymer forming O-rich functional groups.
Hydrophilicity is improved dramatically











Photoelectron spectrum gives composition in few nm thick film







ToF-SIMS shows extremely high concentration of O-rich functional groups on the very surface







Even a brief treatment by oxygen plasma prevents activation of blood platelets



PET foils are used instead of real vascular grafts for quantification





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Another approach: coating of polymer surface with heparin







polyethylene terephthalate (PET) surface is functionalized with amono groups

Nitrogen plasma: N_2 is transformed to N_2^+ , N_2^* , N, N*etc







Plasma 480	

Compositi	on af(er pla	sma	
treatment	С	Ν	Ο	
untreated	74.7		25.3	
NH ₃	64.7	10.6	24.7	
NH ₃ +Ar	65.8	9.6	24.5	
N ₂	61.2	2.9	35.8	
N_2 - H_2	64.5	4.2	31.4	



Best results are obtained by ammonia plasma treatment

NH groups are created in amonia plasma





High-resolution C1s XPS peak cannot reveal amino groups







One can calculate concentration of amino groups from measured Cl content





urface composition after derivatization					
	C	Ν	Ο	Cl	
NH ₃	69.9	3.5	24.8	1.9	
NH ₃ /Ar	70.2	3.0	24.5	2.3	
N ₂	65.0	1.4	33.1	0.5	
N ₂ -H ₂	66.6	2.1	30.5	0.8	

Power (W)	NH_2 /%
untreated	0,4
75 W	3,8
100 W	3,4
150 W	3,7
200 W	3,7
250 W	3,1
$NH_3 + Ar$	4,3
N_2	0,8
$\overline{\mathbf{N}_2} + \mathbf{H}_2$	1,3

XPS gives average values over thickness about 5 nm

Surface is saturated with NH₂ groups after plasma treatment

Amino-groups conc. up to around 4%





Functionalized PET was incubated with heparin



Ultra-thin layer of heparin is formed







Optical microscopy for untreated (left) and treated (right) PET





Incubation with human umbilical vein endothelial cells (HUVEC)





Samples coated by heparin allow for improved adhesion of HUVEC cells





Incubation with human microvascular endothelial cells (HMVEC)



M. Kolar, A. Vesel, M. Modic, I. Junkar, K. Stana-Kleinschek, M. Mozetic,

Method for immobilization of heparin on a polymeric material:

patent application number GB 1416593.0. London: Intellectual Property Office (2014)

Extremely poor adhesion on untreated substrates



Conclusions:

- Vascular grafts made from PET have excellent mechanical and chemical properties but poor hemocompatibility
- Nanostructuring + functionalization with polar groups helps
- Best results are obtained by covalent bonding of heparin
- NHx radicals from ammonia plasma allow for functionalization of PET with amino groups
- Endothelization is improved







Most results taken from theses:

- Martina Modic, Hemostatic response of plasma treated artificial grafts (2012)
- Metod Kolar, Modification of PET biocompatibility by immobilisation of heparin (2015)

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